

Unsteady Flow of Micropolar Fluid through a Circular Pipe under a Transverse Magnetic Field with Suction/Injection

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Abstract. In this paper, we consider the unsteady flow of an incompressible electrically conducting micropolar fluid through a circular porous pipe subjected to periodic suction/injection at the walls of the tube and in the presence of a transverse magnetic field. Under the Stokesian assumption and using the similarity transformations, the stream function and microrotation components are obtained in terms of Bessel's functions. The variation of skin friction with respect to micropolar parameters and Hartman's number, suction parameter are studied and depicted through graphs.

Key words: Micropolar fluid, circular cylinder, MHD, Suction/Injection, Skin friction

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Nomenclature:

a	Radius of the cylinder
\bar{B}_0	Applied magnetic field
c	Cross viscosity parameter $(\kappa/(\kappa + \mu))$
\bar{E}	Electric field
\bar{J}	Current density
j	Microgyration
M	Hartmann number $\left(M = B_0 a \sqrt{\eta/(\mu + \kappa)}\right)$
p	Pressure
\bar{q}	Velocity vector
r	Radial distance
s	Couple stress parameter $(\kappa a^2/\gamma)$
Re	Suction Reynolds number $(\rho V_0 a/(\mu + \kappa))$

t	Time
$u(r, z), w(r, z)$	Velocity components
U_0	Entrance velocity
V_0	Suction velocity
ϵ	Gyration parameter $(\rho j \Omega a^2 / \gamma)$
η	Electrical conductivity
μ'	Magnetic permeability
Ω	Suction frequency
$\mu, \kappa, \alpha, \beta, \gamma$	Material constants (viscosity coefficients)
\bar{v}	Microrotation vector
$v(r, z)$	Microrotation component
σ	Frequency parameter $(\Omega a / V_0)$

1. Introduction

The study of unsteady flow in a porous channel or tubes has received much attention in recent years because of its various applications in biomedical engineering as well as in many other engineering areas such as transpiration cooling gaseous diffusion technology, cooling of rocket etc. The steady flow in a straight channel with porous walls was first studied by Berman [1]. He gave a series solution for the laminar two dimensional flow between two parallel porous plates driven by uniform injection and suction. The problem of finding a similarity solution, by using an analytic perturbation method, of the steady flow in a straight tube with circular cross section was first treated by Yuan *et al* [2]. Terrill [3,4] gave an exact solution for the laminar flow in a pipe of circular cross section. The same problem was studied by Tsangaris and Kondaxakis [5] for unsteady wall suction and/injection.

In recent years, the flows of fluids between parallel plates or tubes have received new attention within the more general context of magnetohydrodynamics (MHD). Terill and Srestha [6] studied the laminar flow between parallel plates in the presence of a magnetic field. Attia and Kotb [7] studied the MHD flow between parallel plates with heat transfer. The study of non-Newtonian fluid flows has gained much attention by the researchers because of their applications in biology, physiology, technology and industry. In addition, the effects of magnetic field on the non-Newtonian fluid also have great importance in engineering applications; for instance, MHD generators, accelerators, aerodynamics heating, electrostatic precipitation, polymer technology, petroleum industry, purification of crude oil and fluid droplets sprays, plasma studies and geothermal energy excitations etc. El-Sakka and El-Dabe [8] have studied the unsteady MHD flow of elastico-viscous fluid in a circular pipe. Moustafa El-Shahed [9] considered the effect of a transverse magnetic field on the unsteady flow of a generalized second grade fluid through a porous medium in a circular tube. Attia [10] has investigated the unsteady flow of a dusty non-Newtonian Bingham fluid through a circular pipe. Khan et al [11] have obtained an exact solution for the MHD flow of a generalized Oldroyd-B fluid in a circular pipe.

The theory of micropolar fluids initiated by Eringen [12] exhibits some microscopic effects arising from the local structure and micro motion of the fluid elements. Further, they can sustain couple stresses and include classical Newtonian fluid as a special case. These fluids can support stress moments and body moments and are influenced by spin inertia. Several investigators have made theoretical study of micropolar fluid flow in the presence of a transverse magnetic field. Kasiviswanathan and Gandhi [13] have studied a class of exact solutions for the MHD flow of a micropolar fluid confined between two infinite, insulated, parallel, non-coaxially rotating disks. Ahmadi and Shahinpoor [14] have studied the criteria for universal stability of the unsteady motion of an incompressible, electrically conducting linear micropolar fluid. Rama Bhargava *et al.* [15] have analyzed the effect of temperature dependent heat sources on the fully developed free convection electrically conducting micropolar fluid between two parallel porous vertical plates in a strong cross magnetic field. In this paper we consider the unsteady flow of an incompressible micropolar fluid through a circular tube with porous wall in the presence of a transverse magnetic field.

2. Formulation of the Problem

Consider the flow of an incompressible electrically conducting micropolar fluid through a porous circular pipe of radius a along the direction of axis of the tube. Assume that there is a periodic suction or injection velocity $V_0 e^{i\Omega t}$ at the wall of the tube. Choose the cylindrical polar coordinate system (r, θ, z) with the origin at the center of the tube and z -axis along the axis of the tube. The flow is subjected to a constant magnetic field \bar{B}_0 perpendicular to the wall and no external electric field is applied. Assume that the magnetic Reynolds number is very small, so that induced magnetic field and electric field produced by the motion of the electrically conducting fluid are negligible. Under the above assumption and using Stokes approximation the equations governing the incompressible MHD micropolar flow in the absence of body forces and body couples are given by

$$(1) \quad \text{div } \bar{q} = 0$$

$$(2) \quad \rho \frac{\partial \bar{q}}{\partial t} = -\text{grad } p + \kappa \text{curl } \bar{v} - (\mu + \kappa) \text{curl } \text{curl } \bar{q} + \bar{J} \times \bar{B}_0$$

$$(3) \quad \rho j \frac{\partial \bar{v}}{\partial t} = -2\kappa \bar{v} + \kappa \text{curl } \bar{q} - \gamma \text{curl } \text{curl } \bar{v} + (\alpha + \beta + \gamma) \text{grad } \text{div } \bar{v}$$

where \bar{q} is the velocity vector, \bar{v} is the micro rotation vector and p is the fluid pressure, ρ and j are the fluid density and micro gyration parameter, \bar{B}_0 is the

magnetic field and \bar{J} is the current density. $\mu, \kappa, \alpha, \beta$ and γ are the material constants (viscosity coefficients) which satisfy the following inequalities.

$$(4) \quad 2\mu + k \geq 0, \quad k \geq 0, \quad 3\alpha + \beta + \gamma \geq 0, \quad \gamma \geq |\beta|$$

The current density \bar{J} , applied magnetic field \bar{B}_0 and electric field \bar{E} are related by Maxwell's equations

$$(5) \quad \begin{aligned} \text{curl} \bar{E} &= -\frac{\partial \bar{B}_0}{\partial t}, \quad \text{div} \bar{B}_0 = 0, \quad \text{curl} \bar{B}_0 = \mu' \bar{J}, \\ \text{div} \bar{J} &= 0 \quad \bar{J} = \eta(\bar{E} + \bar{q} \times \bar{B}_0) \end{aligned}$$

where η is Electrical conductivity and μ' is magnetic permeability. Since the flow is symmetric all the quantities are independent of θ . We choose velocity vector \bar{q} and micro rotation \bar{v} in the form

$$(6) \quad \bar{q} = \{u(r, z)\bar{e}_r + w(r, z)\bar{e}_z\}e^{i\Omega t}, \quad \bar{v} = \frac{v(r, z)}{r}\bar{e}_\theta e^{i\Omega t}$$

Substituting Eq. (6) in Eqs.(1) - (3), we get

$$(7) \quad \frac{\partial u}{\partial r} + \frac{u}{r} + \frac{\partial w}{\partial z} = 0$$

$$(8) \quad \rho\Omega u = -\frac{\partial p}{\partial r} - \frac{\kappa}{r} \frac{\partial v}{\partial z} + (\mu + \kappa) \frac{\partial}{\partial z} \left(\frac{\partial u}{\partial z} - \frac{\partial w}{\partial r} \right) - \eta B_0^2 u$$

$$(9) \quad i\rho\Omega w = -\frac{\partial p}{\partial z} + \frac{\kappa}{r} \frac{\partial v}{\partial z} - \frac{(\mu + \kappa)}{r} \frac{\partial}{\partial r} \left(r \left(\frac{\partial u}{\partial z} - \frac{\partial w}{\partial r} \right) \right) - \eta B_0^2 w$$

$$(10) \quad i\rho\Omega jv = -2\kappa v + \kappa \frac{\partial u}{\partial z} - \frac{\partial w}{\partial r} + \gamma E^2 v$$

where $E^2 = \frac{\partial^2}{\partial r^2} - \frac{1}{r} \frac{\partial}{\partial r} + \frac{\partial^2}{\partial z^2}$ is the Stokes operator. The boundary conditions are

$$(11) \quad \begin{aligned} u(r, z) &= V_0, \quad w(r, z) = 0 \quad \text{and} \quad v(r, z) = 0 \quad \text{at} \quad r = a \\ u(r, z) &= 0, \quad \frac{\partial w}{\partial r} = 0 \quad \text{at} \quad r = 0 \quad \text{and} \quad \frac{v(r, z)}{r} = 0 \quad \text{as} \quad r \rightarrow 0 \end{aligned}$$

Introducing the following non-dimensional scheme

$$(12) \quad r = a\tilde{r}, \quad w = V_0\tilde{w}, \quad u = V_0\tilde{u}, \quad v = V_0\tilde{v}, \quad p = \rho V_0^2 \tilde{p}, \quad t = \frac{a\tilde{t}}{V_0}$$

and the stream function $\psi(r, z)$ through,

$$(13) \quad u(r, z) = \frac{1}{r} \frac{\partial \psi}{\partial z} \text{ and } w(r, z) = -\frac{1}{r} \frac{\partial \psi}{\partial r}$$

in to the Eqs. (8) - (9) and eliminating pressure from the resulting equations, we get (after dropping tildes)

$$(14) \quad i\sigma Re E^2 \psi = -c E^2 v + E^4 \psi - M^2 E^2 \psi$$

$$(15) \quad (2s + i\epsilon)v = s E^2 \psi + E^2 v$$

where, $c = \frac{\kappa}{\kappa + \mu}$ is the cross viscosity parameter, $s = \frac{\kappa a^2}{\gamma}$ is the couple stress parameter, $Re = \frac{\rho V_0 a}{\mu + \kappa}$ is the Suction Reynolds number $\sigma = \frac{\Omega a}{V_0}$ is the frequency parameter, $\epsilon = \frac{\rho j \Omega a^2}{\gamma}$ is the gyration parameter, $M = B_0 a \sqrt{\frac{\eta}{\mu + \kappa}}$ is the Hartmann number corresponding to micropolar fluid. From Eq. (14) and Eq. (15) we have

$$(16) \quad v = -\frac{M^2 + i\sigma Re}{c\lambda_1^2 \lambda_2^2} [E^4 \psi - (\lambda_1^2 + \lambda_2^2) E^2 \psi] - E^2 \psi$$

Substituting v in Eq. (14) we get

$$(17) \quad E^2(E^2 - \lambda_1^2)(E^2 - \lambda_2^2)\psi = 0$$

where

$$(18) \quad \lambda_1^2 + \lambda_2^2 = (2 - c)s + M^2 + i(\sigma Re + \epsilon)$$

$$(19) \quad \lambda_1^2 \lambda_2^2 = (2s + i\epsilon)(M^2 + i\sigma Re)$$

3. Solution of the Problem

Following Terril [3], we can write the stream function and microrotation components as

$$(20) \quad \psi = \left(\frac{U_0}{V_0} - z \right) F(r) \quad \text{and} \quad v = \left(\frac{U_0}{V_0} - z \right) G(r)$$

$F(r)$ and $G(r)$ are functions of r to be determined and U_0 average entrance velocity.

Substituting Eq. (20) in Eq. (16) and Eq. (18) we get

$$(21) \quad D^2(D^2 - \lambda_1^2)(D^2 - \lambda_2^2)F = 0$$

$$(22) \quad G(r) = -\frac{M^2 + i\sigma Re}{c\lambda_1^2\lambda_2^2}[D^4F - (\lambda_1^2 + \lambda_2^2)D^2F] - D^2F$$

where $D^2 = \frac{d^2}{dr^2} - \frac{1}{r} \frac{d}{dr}$

The boundary conditions in terms of F and G are

$$(23) \quad \begin{aligned} F(1) = 1, \quad F'(1) = 0, \quad G(1) = 0, \quad F(0) = 0, \\ D^2F = 0 \quad \text{at} \quad r = 0 \quad \text{and} \quad \frac{G(r)}{r} = 0 \quad \text{as} \quad r \rightarrow 0 \end{aligned}$$

The general solution of Eq. (21) is

$$(24) \quad F = a_1 + a_2r^2 + a_3rI_1(\lambda_1r) + a_5rK_1(\lambda_1r) + a_4rI_1(\lambda_2r) + a_6rK_1(\lambda_2r)$$

where a_1, a_2, a_3, a_4, a_5 and a_6 are arbitrary constants and $I_1(\lambda_1r)$ and $K_1(\lambda_1r)$ are modified Bessel functions of the first-order of first and the second kind respectively. Substituting F in Eq. (20), we get

$$(25) \quad \begin{aligned} cG = (M^2 + i\sigma Re - \lambda_1^2)[a_3rI_1(\lambda_1r) + a_5rK_1(\lambda_1r)] \\ + (M^2 + i\sigma Re - \lambda_2^2)[a_4rI_1(\lambda_2r) + a_6rK_1(\lambda_2r)] \end{aligned}$$

Using the boundary conditions (23) we get

$$(26) \quad a_1 = a_5 = a_6 = 0$$

$$(27) \quad a_2 + \frac{\lambda_1}{2}[I_2(\lambda_1) + I_0(\lambda_1)]a_3 + \frac{\lambda_2}{2}[I_2(\lambda_2) + I_0(\lambda_2)]a_4 = -1$$

$$(28) \quad a_2 + a_3I_1(\lambda_1) + a_4I_1(\lambda_2) = 1$$

$$(29) \quad a_3(M^2 + if - \lambda_1^2)I_1(\lambda_1) + a_4(M^2 + if - \lambda_2^2)I_1(\lambda_2) = 0$$

Solving these equations the constants a_2, a_3, a_4 can be obtained.

4. Pressure Distribution

From Eq. (8) and Eq. (9), the non dimensional pressure is given by

$$(30) \quad \begin{aligned} Re \frac{\partial p}{\partial r} &= \frac{1}{r} [-(M^2 + i\sigma Re)F + cG + D^2 F] \\ Re \frac{\partial p}{\partial z} &= \frac{(\frac{U_0}{V_0} - z)}{r} [-(M^2 + i\sigma Re)F' + cG' + \frac{d}{dr} D^2 F] \end{aligned}$$

On integrating Eq. (30) and after simplification we have

$$(31) \quad Re p = -(M^2 + i\sigma Re) \left\{ \frac{r^2}{2} + \left(\frac{U_0}{V_0} - z \right)^2 \right\} a_2 + p_0$$

5. Skin Friction

The stress tensor t_{ij} for micropolar fluid is given by

$$(32) \quad t_{ij} = (-p + \lambda \text{div} \bar{q}) \delta_{ij} + (2\mu + \kappa) e_{ij} + \kappa \epsilon_{ijm} (\omega_m - v_m)$$

where v_i and $2\omega_i$ are the components of the microrotation vector and the vorticity vector respectively, e_{ij} are the components of the rate of strain, ϵ_{ijm} is the alternating symbol and comma denotes covariant differentiation.

The shear stress T_{rz} is given by

$$(33) \quad T_{rz} = \frac{V_0(\mu + \kappa)}{r a^2} \left(\frac{U_0}{V_0} - z \right) (-D^2 F + cG)$$

Hence the coefficient of skin friction $C_f (= 2T_{rz}/\rho V_0^2)$ on the wall of the cylinder $r = 1$ is given by

$$(34) \quad C_f = \frac{(M^2 + i\sigma Re)}{Re} \{a_2 I_1(\lambda_1) + a_3 I_1(\lambda_2)\}$$

6. Results and Discussions

The system of equations (26) - (29) is solved using MATHEMATICA and the stream function ψ in Eq. (20) is calculated from Eq.(24). Then the flow pattern is obtained for different times at $\pi/4$, $\pi/2$, π and $3\pi/2$ over a cycle of suction by taking real part of $\psi e^{i\sigma\tau}$ and is shown in Fig.2. As it is expected, the figure shows that the flow is of oscillatory nature over a period 2π .

To explicitly see the effects of various parameters like cross viscosity parameter (c), couple stress parameter (s), suction Reynolds number (Re), magnetic parameter (M), gyration parameter (ϵ) and frequency parameter (σ) on the skin

friction (shear stress at the wall), coefficient of skin friction given in Eq. (34) is numerically evaluated and the results are graphically presented in Figs. 3 -7. If $\sigma \neq 0$, then the geometric parameters λ_1 and λ_2 are complex which are not conjugate to each other. If one of the values of λ_1 and λ_2 is real, the other value need not be real. Hence the velocity field, microrotation field and skin friction are complex. The real parts of these quantities i.e. when suction is in the form of a cosine oscillation are taken and the skin friction is numerically evaluated. The effect of couple stress parameter s on the skin friction is shown in Fig. 3 for $\epsilon = 5, c = 0.4, Re = 0.6, M = 10$, and $\sigma = 10$. It can be observed that as the couple stress parameter s increases, the skin friction is decreasing. In the limit as $s \rightarrow \infty$ (i.e. $\gamma \rightarrow 0$ and $\kappa \rightarrow 0$), the governing equations (8-10) reduce to the corresponding equations for a viscous fluid. Hence, viscous fluids have less skin friction compared to that of micropolar fluids. This is expected because of the rotational motion arising from the micromotion of the fluid molecules in micropolar fluids. Similarly as cross viscosity parameter c increases the skin friction is decreasing. The variation of skin friction with c for different values of ϵ is given in Fig. 4 for the values of $s = 15, c = 0.4, Re = 0.6, M = 10$ and $\sigma = 10$. It can be seen from this figure that as the gyration parameter ϵ increases, the skin friction is decreasing. When ϵ increases, radius of the volume element increases or angular velocity of the particle decrease and hence skin friction decreases.

Fig. 5 shows the effect of suction Reynolds number Re on the skin friction for the values of $\epsilon = 5, c = 0.4, s = 15, M = 10$ and $\sigma = 10$. It is interesting to note that as the suction velocity increases (i.e Re increases), the skin friction is decreasing. This observation is similar to that of viscous fluids. There is sudden decrease from 58 to 20 in the value of the skin friction when the value of Re is increased from 0.2 to 0.6. Hence the skin friction is very sensitive to the suction Reynolds number.

The effect of the magnetic parameter (M) on the skin friction is shown in Fig. 6 for the values of $\epsilon = 5, c = 0.4, s = 15, Re = 0.4$, and $\sigma = 10$. It can be noted from this figure that skin friction increases with the increase in magnetic parameter M . This happens because of the imposing of a magnetic field normal to the flow direction. This magnetic field gives rise to a resistive force and slows down the movement of the fluid. The variation of skin friction with frequency parameter is shown in Fig. 7 for $\epsilon = 5, c = 0.4, s = 15, Re = 0.4$, and $M = 10$. It is clear from this figure that the skin friction is increasing with the frequency parameter increases.

7. Conclusions

The flow generated in a circular cylinder due to periodic suction/injection applied on the wall of the tube under a constant magnetic field is considered. It can be noted that applied suction at the surface and the couple stress parameter decreases the skin friction. Where as the frequency of suction, the gyration parameter and the magnetic field increases the skin friction.

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Figures

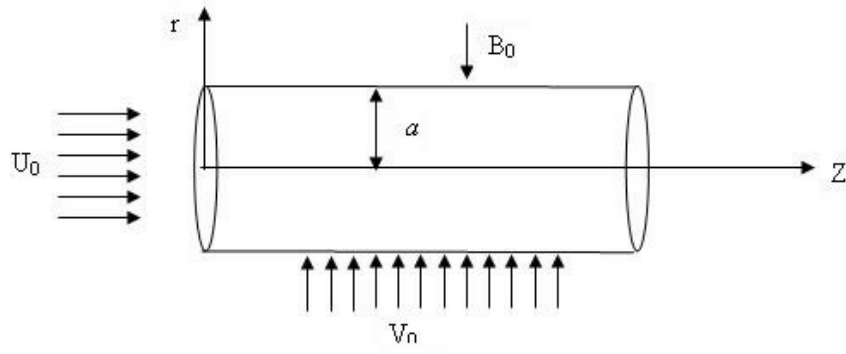
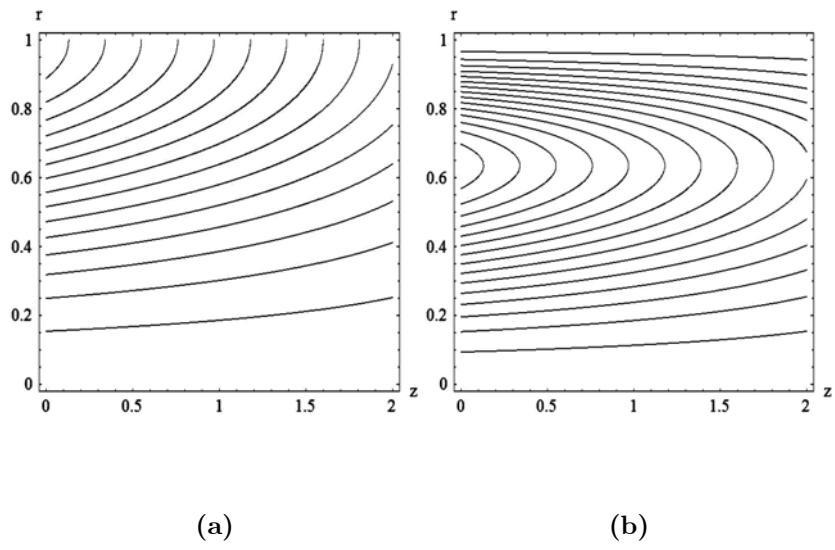


Figure 1. Schematic diagram



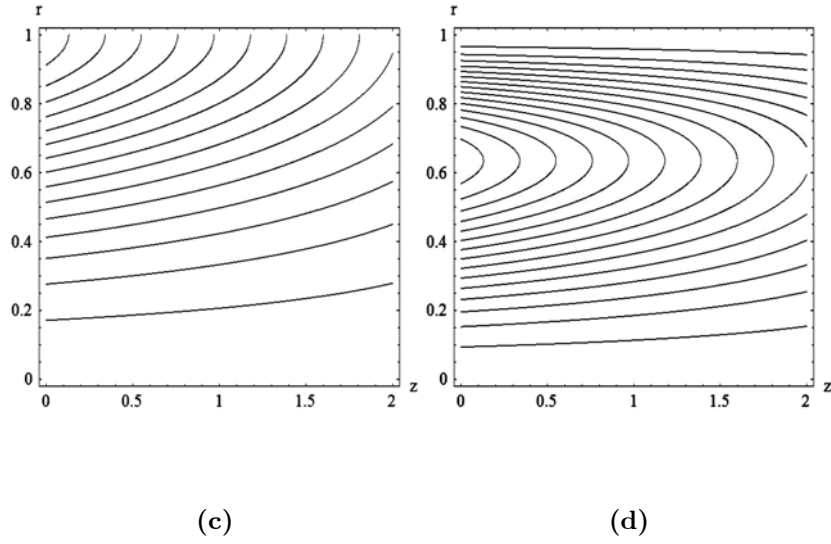


Figure 2. Stream lines above the centre line of the pipe for $\epsilon = 5$, $c = 0.4$, $s = 15$, $Re = 0.6$, $M = 10$, $\sigma = 10$ at time (a) $\tau = \pi/4$, (b) $\tau = \pi/2$, (c) $\tau = \pi$ (d) $\tau = 3\pi/2$.

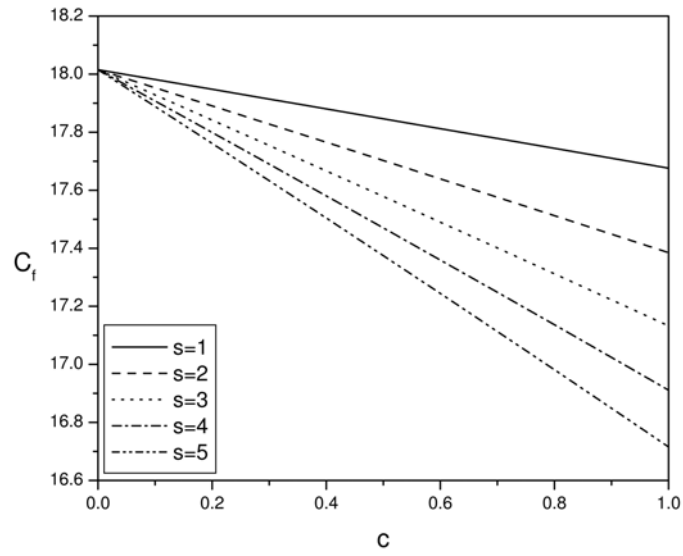


Figure 3. Variation of skin friction with couple stress parameter s for $\epsilon = 5$, $c = 0.4$, $Re = 0.6$, $M = 10$, $\sigma = 10$

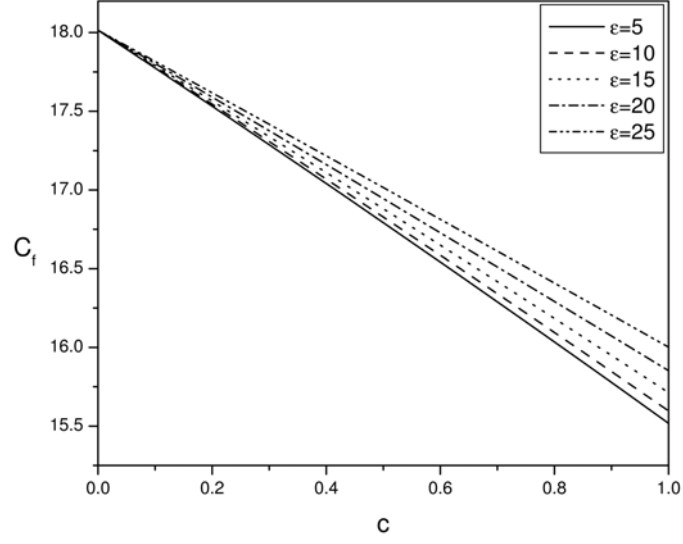


Figure 4. Variation of skin friction with gyration parameter ϵ for $s = 15$, $c = 0.4$, $Re = 0.6$, $M = 10$, $\sigma = 10$

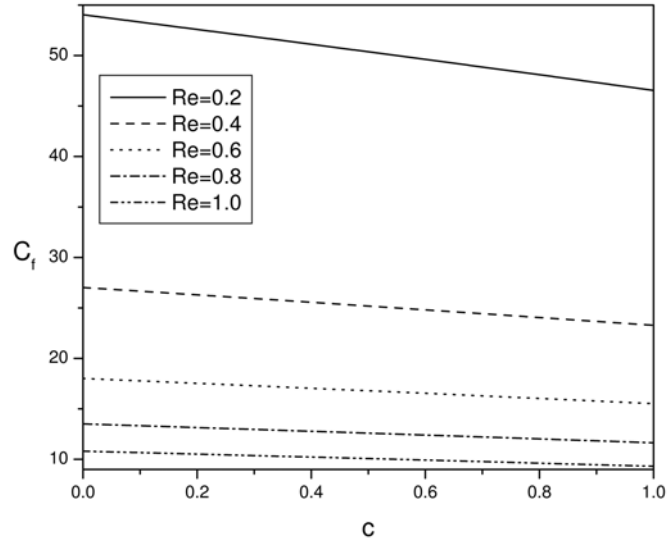


Figure 5. Variation of skin friction with Suction Reynolds number Re for $\epsilon = 5$, $c = 0.4$, $s = 15$, $M = 10$, $\sigma = 10$

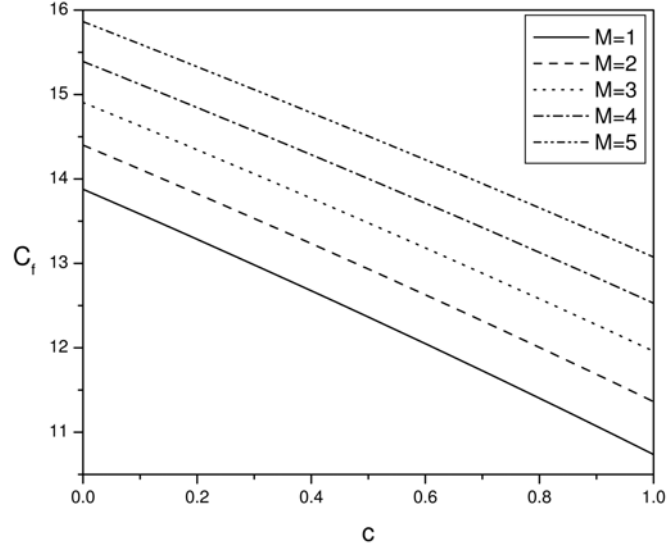


Figure 6. Variation of skin friction with Hartmann number M for $\epsilon = 5$, $c = 0.4$, $Re = 0.6$, $s = 15$, $\sigma = 10$

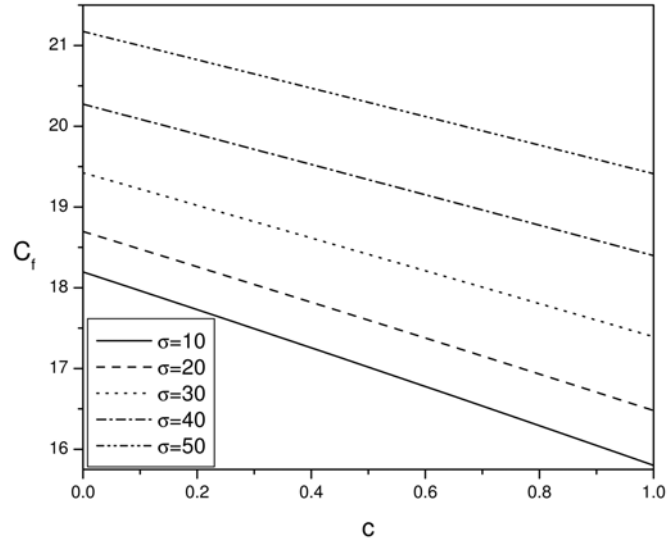


Figure 7. Variation of skin friction with frequency parameter σ for $\epsilon = 5$, $c = 0.4$, $Re = 0.6$, $M = 10$, $s = 15$